Significance of connective tissue proliferation in the breakdown of cartilage: a novel in vivo model

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SUMMARY The implantation of homologous femoral head cartilage in subcutaneous tissues of random bred Wistar rats results in both subchondral and articular surfaces becoming overlaid by an adherent granulation tissue comprising predominantly fibroblast-like cells. The response of the tissue to cartilage encapsulated with cotton fibres was also similar but erosions, mainly subchondral, were more evident and proteoglycan loss markedly greater. The connective tissue response to cotton was the progressive formation of a foreign body granuloma comprising mononuclear cells, multinucleated giant cells, and fibroblasts with very few polymorphonuclear leucocytes.

Rheumatoid arthritis is a chronic inflammatory disorder in which bone and cartilage of articulating joints are slowly destroyed by a proliferating invasive granulomatous tissue called pannus. This is derived from the synovial membrane and its microvasculature and is histologically characterised by proliferating fibroblasts, variable numbers of macrophages, lymphocytes, and plasma cells, blood vessels, and occasional collagen fibres. Destruction of cartilage is believed to be caused by degradative enzymes produced by cells of the pannus and by cartilage. This has been borne out from studies conducted in vitro, which have shown that macrophages, fibroblasts, and chondrocytes can release connective tissue degrading enzymes and inflammatory mediators and can cause the loss of matrix from cartilage explants. These studies have also shown that both fibroblast and chondrocyte cell activities can be increased significantly after interacting with a macrophage derived factor, interleukin 1.

The need for in vivo models to improve our understanding of the process of cartilage breakdown and in the search for new therapeutics has recently been stressed by Rainsford. We have attempted this over the past few years by studying cartilage breakdown after implantation into preformed subcutaneous air pouches in rodents. These pouches bear cavity linings resembling synovial tissue in structure, ultrastructural appearance, histochemical properties, phagocytic ability, and response to injury. Matrix loss from cartilage implants, however, was not influenced either by inflammation of the cavity or by implantation in non-inflated subcutaneous tissues.

More recently we have studied the effect of varying the way in which inflammation and soft tissue is presented to cartilage and have investigated the effect of implanting cartilage in close association with cotton. Implantation of cotton in subcutaneous tissues of rodents is known to stimulate a granulomatous inflammation concomitant with the growth of granulation tissue. We have found that cartilage proteoglycan loss is accelerated in its presence, and we report on this and speculate on the mechanisms contributing to this breakdown.

Materials and methods

Animals

Random bred Wistar strain rats weighing 150–200 g of both sexes were used. These were obtained from a colony maintained by the animal house at St Bartholomew's Hospital. Male rats were used for all experiments. Female rats were used only as donors of cartilage.
ISOLATION OF FEMORAL HEAD CARTILAGE

Rats were killed by cervical dislocation and the skin overlying the hip joint swabbed with alcohol, then excised. The joint was palpated through the overlying gluteus maximus muscle and an incision made across the muscle, cutting a flake of bone from the greater trochanter and dividing the capsular ligament to expose the neck of the femur. Pressure was then applied to the upper leg to dislocate the joint. Tere's ligament was divided and the cartilage cap eased from the femoral head with bone cutters. The cartilages were kept at room temperature in minimum essential medium containing 200 U/ml penicillin (Gibco) and 1-0 mg/ml streptomycin (Gibco) and implanted within one hour of collection.

IMPLANTATION OF CARTILAGE AND COTTON; ASSESSMENT OF GRANULOMATOUS RESPONSE

A modification of the method of Meier et al of implanting cotton subcutaneously was used. Sterile rectangular (0.5x0.75 cm) pieces of cotton of equal weight and roughly equal surface area and thickness were wrapped firmly around cartilages and allowed to soak in antibiotic supplemented medium for a short time before implanting subcutaneously in one flank of the rats. Cartilages treated similarly but without cotton were implanted in the opposite flank. At varying time intervals after implantation the rats were killed and the implants removed. Cartilage was assayed for proteoglycan as described below. Where cotton was implanted this was dissociated from the cartilage and immediately weighed (wet weight). The cotton was subsequently reweighed after drying at 37°C for 72 h. The granulomatous response induced at the site of implantation was assessed by determining the amount of water (exudate=wet weight of cotton−dry weight of cotton) and granulation tissue (dry weight of cotton−original weight of cotton) accumulating in the cotton.

DETERMINATION OF CARTILAGE PROTEOGLYCAN

Cartilage proteoglycan was determined by the method of Farndale et al. Cartilages were digested with papain (type III; Sigma Chemical Co) in a digestive buffer for two hours at 55°C and the digest reacted with 1,9-dimethylmethylene blue for spectrophotometry. Absorbance values at 535 nm were then compared with a chondroitin sulphate (Sigma Chemical Co) standard curve.

HISTOLOGY

Cartilage implants with associated tissues were fixed in 10% formal saline and 5 μm paraffin sections prepared. Sections were stained with Harris' haematoxylin and eosin.

Results

MICRO-AND MACROSCOPIC FEATURES OF SUBCUTANEOUS IMPLANTS

Four days after implantation into subcutaneous tissues of rats the femoral heads with (2 mg) and without cotton could be easily separated from surrounding connective tissue. There were no signs of haemorrhage or necrosis of tissue adjacent to the implants. After four days the implants became

Fig. 1 Femoral head cartilage implant in subcutaneous tissues eight days after implantation.
progressively bound by connective tissue; those with cotton were more adherent and rigidly held in position by thickening connective tissue on either side. Although the cotton encapsulates could be easily dissociated after the fourth day of implantation, this became increasingly difficult as the duration of implantation increased; implants became firmly encapsulated with granulomatous tissue but there were no macroscopic signs of invasion into cartilage and generally these were recovered intact.

A histological examination of the implants showed that at four days cartilage without cotton was surrounded by connective tissue having the histological appearance of granulation tissue. This was composed of layers of predominantly fibroblast-like cells with interspersed mononuclear cells and capillaries (Fig. 1). The thickness of this tissue varied considerably (approx. 50–100 µm). Some pigmented cells, presumably haemosiderin laden macrophages, were also seen. Characteristically the tissue was closely packed and adherent to the articular surface of the implanted cartilage but showed less organisation adjacent to the subchondral areas. The nature of the granulation tissue did not appear to alter significantly when examined at later times.

The connective tissue response to cotton-cartilage implants showed three distinct zones (Fig. 2). Immediately adjacent to the cartilage was a layer of granulation tissue resembling the response seen to cartilage implanted without cotton. Surrounding this was a foreign body granuloma of fibroblasts, mononuclear cells, giant cells, and focal areas of degenerating polymorphonuclear leucocytes. The outermost zone was again a layer of granulation tissue. At day 4 parts of the granuloma, particularly nearer the cartilage, appeared relatively acellular. By day 8 the granuloma appeared to have matured and did not alter histologically at later times.

Cartilage erosions were more extensive in cotton-cartilage implants than in cartilage implanted alone. The pattern of erosions in both cases was, however, similar. Erosions were seen from day 8 onwards and increased in extent with time. In the main the articular surface of implants remained intact with just a few local erosions. The exception to this occurred when there was clear evidence that Tere's ligament had been torn away from its insertion site and given access to invading cells. Most erosions were seen to occur from the subchondral side of the implants, destroying usually the layer of calcified chondrocytes. In cotton implants this process was complete by about day 12; in non-cotton implants it was not always complete at the end of the study. The invading cells had the character of the granulation tissue cells surrounding each cartilage implant. The subchondral side of the articular hyaline cartilage appeared to be spared major erosions. In general the chondrocytes of the epiphyseal disc and the articular hyaline cartilage seemed to be viable throughout the study (Figs 1 and 2).

**PROTOGLYCAN LOSS FROM CARTILAGE IMPLANTS**

The proteoglycan content of cartilages in the flanks of rats during the implantation period is shown in Fig. 3. Proteoglycan loss occurred sooner from implants wrapped with cotton (2 mg), beginning

![Fig. 2. Femoral head cartilage in cotton granuloma in subcutaneous tissues eight days after implantation.](http://ard.bmj.com/Downloaded from http://ard.bmj.com/ on June 25, 2017 - Published by group.bmj.com)
De Brito, Moore, Adhya, Al-Duaij, Willoughby
tour to eight days after implantation and reaching a maximum loss 12 to 16 days later. After 24 days the total loss of proteoglycan from both implants was the same.

In another experiment the effect of increasing the weight of cotton around the cartilage was investigated (Fig. 4). After the first week of implantation there was a significant reduction in the proteoglycan content of cartilages bearing cotton, regardless of weight. By the second week only the cartilage wrapped with 2 mg of cotton had a significantly lower proteoglycan content than the cotton free control cartilage in the opposite flank. The proteoglycan content of the cotton free cartilages implanted in animals having 4 and 8 mg of cotton was much lower (but not significantly) than that of the group having 2 mg of cotton added to implant.
cotton and the group with no cotton. There was, however, an increase in the accumulation of inflammatory fluid and the formation of granulation tissue in the implants after one and two weeks which was related to the weight of the cotton (Fig. 5).

Discussion

The present study confirms in vitro observations on the contribution made by mononuclear cells and fibroblasts in the destruction of cartilage. Homologous femoral head cartilage implanted subcutaneously in rats developed fewer surface erosions and lost less proteoglycan than similar cartilage implants encapsulated with cotton. Both implants, however, became enveloped by a granulation tissue composed predominantly of layers of fibroblasts, but the principal difference between the two was the distinctive granulomatous cellular response beneath induced by cotton. Mononuclear and multinucleated giant cells were part of this response. In this respect the connective tissue response elicited by cotton could be similar to that induced by pannus in the early phase of rheumatoid arthritis, as described by Shiozawa et al. These workers observed that cartilage became overlaid with fibroblast-like cells before macrophage-like cells which were present beneath began to invade the cartilage. The accelerated breakdown of cartilage produced by cotton would appear to be caused by the granulation tissue activated by humoral and cellular products of the developing granuloma. Immunological mechanisms of rejection may contribute to this breakdown. The role of interleukin 1 in this model of cartilage breakdown is presently being pursued, but the absence of enlarged chondrocyte lacunae after substantial proteoglycan loss would appear to exclude any effect via the chondrocyte.

The articular surface of cartilage implants remained relatively intact throughout the implantation period (24 days). Erosions were commonly found in the subchondral plate, their size and number increasing with time. This contrasts somewhat with the situation in the rheumatoid joint, where although proliferation of granulation tissue at the margins of the joint is an important cause of subchondral erosions, the articular surface is also breached. It is possible that the period of implantation of cartilages in this study may not have been sufficiently long for this to happen. In a

![Graph showing weight of cotton and granulation tissue](http://ard.bmj.com/)

**Fig. 5** Quantitative assessment of the granulomatous response induced by different weights (mg) of cotton after implantation with cartilage in subcutaneous tissues. Cotton-cartilage implants were removed at one and two weeks after implantation. Exudate (water content) = wet weight of cotton−dry weight of cotton; granulation tissue = dry weight of cotton−original weight of cotton. Each result represents the mean ± SEM of six implants. *p<0.05; this result is significantly different from the corresponding 2 mg result.
histological study of the development of arthritis in a spontaneously developing animal model, the MRL/1 mouse, O'Sullivan et al found that the earliest pathological change appearing in joints was synovial cell proliferation in the joint recesses, with associated subchondral bone destruction producing marginal erosions. The articular cartilage was spared during this time, though a few weeks later it was affected. It was interesting that these changes occurred without the presence of subsynovial or periarticular inflammation.

The association of inflammation with destruction of cartilage in rheumatoid arthritis remains a controversial issue. In experimental rodents the implantation of femoral head cartilage in immunologically and non-immunologically inflamed subcutaneous air pouches was not found to accelerate proteoglycan loss. Swingle and Shideman described three phases of the inflammatory response to implanted cotton pellets: a transudative phase (zero to three hours), an exudative phase (three to 72 hours), and a proliferative phase (four days onwards). The first two components were essentially increases in fluid accumulation of the pellet coupled with a large polymorph presence and only a few mononucleated cells. In the proliferative phase polymorph numbers declined and lymphocyte, macrophage, and fibroblast numbers increased. This also coincided with the appearance and increased synthesis of collagen and lysosomal enzymes. The time course of accelerated loss of proteoglycan by cotton correlates with the latter phase and it is possible that this may be due to the increased presence of degradative enzymes. Increasing the weight of cotton, however, did not cause further breakdown of cartilage, suggesting that the intensity of the granulomatous inflammatory process may not be important for cartilage proteoglycan loss. This could be explained by an increased production of proteolytic enzyme inhibitors, which could also account for the fact that cartilages in inflamed air pouches fail to degrade faster. Wrapping cartilages with less than 2 mg of cotton was not possible, consequently limiting a complete cotton dose related study.

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References

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