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In vitro growth of calcium pyrophosphate crystals in polyacrylamide gels

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Pyrophosphate arthropathy is characterised by the presence of microrcrystalline deposits of calcium pyrophosphate (CPPD) in articular tissues. 1 The crystals occur in two crystallographic forms—namely, monoclinic (CPPD(M)) and triclinic (CPPD(T)). No other crystal species of calcium pyrophosphate has been found in vivo.

This is surprising, as in vitro studies performed under simulated physiological conditions most often yield the orthorhombic form of the tetrahydrate, CPPT(O). 2 Although prolonged incubation may yield CPPD(M) and CPPD(T). 2

Crystal deposition in vivo is restricted to pathological hyaline cartilage, fibrocartilage, and synovium and this has led to speculation that the physicochemical properties of connective tissue are important in nucleation and crystal growth. 3 In vitro models, using gelatin and silica hydrogels, have therefore been developed in an attempt to represent the physical properties of the tissue matrix. 3

Using gelatin gels at room temperature we investigated the dependence of the crystal form on the calcium ion concentration and the critical pH. Preliminary studies have revealed local changes in pH accompanying crystal deposition.

The gels were prepared using the method of Pritzker et al., 4 whereby a solution of CaCl₂ is layered on top of the gel, previously soaked overnight in 2-8 mmol Na₃PO₄ and the pH adjusted at 60°C using 0·1 mol NaOH/HCl.

Using 0·2 mol CaCl₂ resulted in the formation of both CPPD(T) and CPPT(O) after a period of three weeks. However, careful concentration programming, by which 0·02 mol CaCl₂ is added to the supernatant daily until nucleation occurs (the solution then being made up to 0·2 mol CaCl₂) yielded only CPPD(T) identified by x-ray powder diffraction. By varying the initial pH of the gel from pH 5·5 to pH 8·5 at 60°C, it was found that growth of CPPD(T) was favoured by slightly alkaline conditions.

The crystal deposits formed in layers within the gel, collectively known as Liesegang rings. Addition of BDH universal indicator revealed an increase in acidity with depth of approximately 3 pH units. This increase was not entirely uniform but altered sharply by up to 0·2 pH units, at the edges of the Liesegang rings. These observations imply that crystal deposition is closely linked to the pH of the immediate surroundings.

A disadvantage of using a gelatin hydrogel as a model system is that it degrades above 30°C to become a viscous liquid and is therefore unsuitable for investigating crystal deposition at physiological temperatures.

We have therefore used a polyacrylamide gel which retains its structural properties even above body temperature.

Preparation of the gel involves mixing equal volumes of 2·8 mmol Na₃PO₄ and 10% w/v polyacrylamide solution (made by dissolving 10 g polyacrylamide and 0·365 g NN'dialkyltartardiamide in 100 ml distilled water). Tetramethyl-ethylene diamine (0·25 µl/10 ml solution) is added and the pH adjusted to between pH 6 and pH 7 with 10 N HCl/NaOH. Polymerisation is induced with 0·25 µl/10 ml solution of ammonium persulphate. After gelation, typically 10–15 minutes, neutral 0·2 mol CaCl₂ is carefully poured on top of the gel, which is then incubated at either room temperature or 37°C for up to three weeks.

After one week small discrete crystallites were observed throughout the gel, although there was no evidence of any Liesegang rings, so prevalent in gelatin gels. The crystallites were extracted by placing the gel into a continuously stirred 2% solution of NaIO₄ for two hours; the crystals were recovered from solution by filtration.

Optical microscopy performed on the crystallites within the gel revealed two essentially different morphologies; one dendritic, the other spheroidal (or in many cases toroidal) hollow shells.

X-ray powder diffraction of crystals grown at room temperature identified the deposits as a mixture of CPPD(T) and CPPT(O), while those crystals deposited at 37°C were found to be pure CPPD(T) within the pH range 6–7.

The pH within the gel appeared not to change during the crystal growth process, unlike the situation in gelatin hydrogels.

Conclusions

We have shown that a low calcium concentration and an alkaline pH favour the growth of CPPD(T) crystals in gelatin gels. Using polyacrylamide gels we have found that the temperature of the growth medium is important in deciding the nature of the crystal form and that at 37°C pure CPPD(T) can be grown.

Gelatin and polyacrylamide gels show considerably different responses to crystal growth in terms of the formation of Liesegang rings and local pH variations. In view of these differences it appears that the gel is intimately involved in the crystal growth process. Therefore, careful studies must be made to ensure that current model systems in use are realistic physiological models for crystal deposition in human articular cartilage.

References

Under simple simulated physiological conditions in vitro we have previously established that 40 μmol/l of pyrophosphate is needed to initiate formation of calcium pyrophosphate crystals in the presence of 1-5 mmol/l of Ca++ at 37°C in three days. If magnesium is added to the system to approach the physiological range (0-5 mmol/l) the requirement for pyrophosphate rises to 175 μmol/l. We have now investigated the effect of another important ion, orthophosphate, over the physiological range, on crystal formation and on long term crystal growth.

Contrary to expectation there was a dose-related decrease in the amount of pyrophosphate needed to initiate the formation of calcium pyrophosphate crystals in the presence of increasing phosphate. At 0-5, 1-0, and 2-0 mmol/l phosphate, 125, 75, and 37-5 μmol/l pyrophosphate are required respectively in the presence of a standard 1-5 mmol/l Ca++ and 0-5 mmol/l Mg++. These results are of particular interest because hitherto it has been thought that pyrophosphate acts as an inhibitor of calcium phosphate crystal deposition. The use of 1 mmol/l phosphate and 1-5 mmol/l of calcium with pyrophosphate added creates conditions that are close to physiological and raises the important question of which crystal forms first deposit in vivo. The amount of pyrophosphate (75 μmol/l) needed for crystal growth of calcium pyrophosphate is still higher than the amount of pyrophosphate found in extracellular fluids (normal range 1-4 μmol/l) or in synovial fluid in pseudogout (range 5-60 μmol/l). This suggests that under pathological conditions in vivo additional mechanisms may be needed to produce high local concentrations of calcium or PP, or that nucleating agents are involved.

Long term incubations at physiological temperature, pH, and ionic strength, with 1-5 mmol/l Ca++, 0-5 mmol/l Mg++ and 200 μmol/l pyrophosphate lead, in the absence of phosphate, to the formation of predominantly monoclinic crystals of calcium pyrophosphate. The addition of phosphate at 1 mmol/l stabilises the amorphous gel that is formed initially, thereby prolonging the time needed for crystal growth. However, it does lead to the formation of much larger crystals. These crystals are of the same type as in the absence of phosphate but differ in that a small proportion of the crystals grow slowly to crystals which appear by optical criteria to be triclinic calcium pyrophosphate dihydrate (the type found in vivo). This indicates that under simulated physiological conditions of pH and ionic strength and at physiological concentrations of key ions, it is possible to grow the crystal type found pathologically by using high (200 μmol/l) pyrophosphate concentrations.

Preliminary results indicate that addition of large numbers of hydroxyapatite crystals (40 μg/ml) raise the concentration of pyrophosphate required for CPP crystal initiation, presumably because they bind pyrophosphate to their surfaces. Lower numbers of added crystals (4 μg/ml) on the other hand had no obvious effect on the initiation of CPP, crystals, suggesting that any surface binding effect was compensated by a promoting effect on nucleation.

In long term incubations (>2 months) neither added hydroxyapatite nor added CPP, crystals altered the type of new CPP, crystals formed. Both types of crystals considerably accelerated CPP, crystal formation in the presence of excess PP, (100-300 μmol/l) both in the presence and absence of phosphate.

In conclusion, it has not yet been possible to grow the pathological CPP, crystal type (triclinic) in short term culture in vivo under simulated physiological conditions. Such crystals do, however, appear in long term incubations (>2 years), supporting the suggestion that their presence in chondrocalcinosis represents the end point of a gradual process.

Reference
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